

Pulse Programming Bootcamp

Day 1: Imaging Sequence Elements

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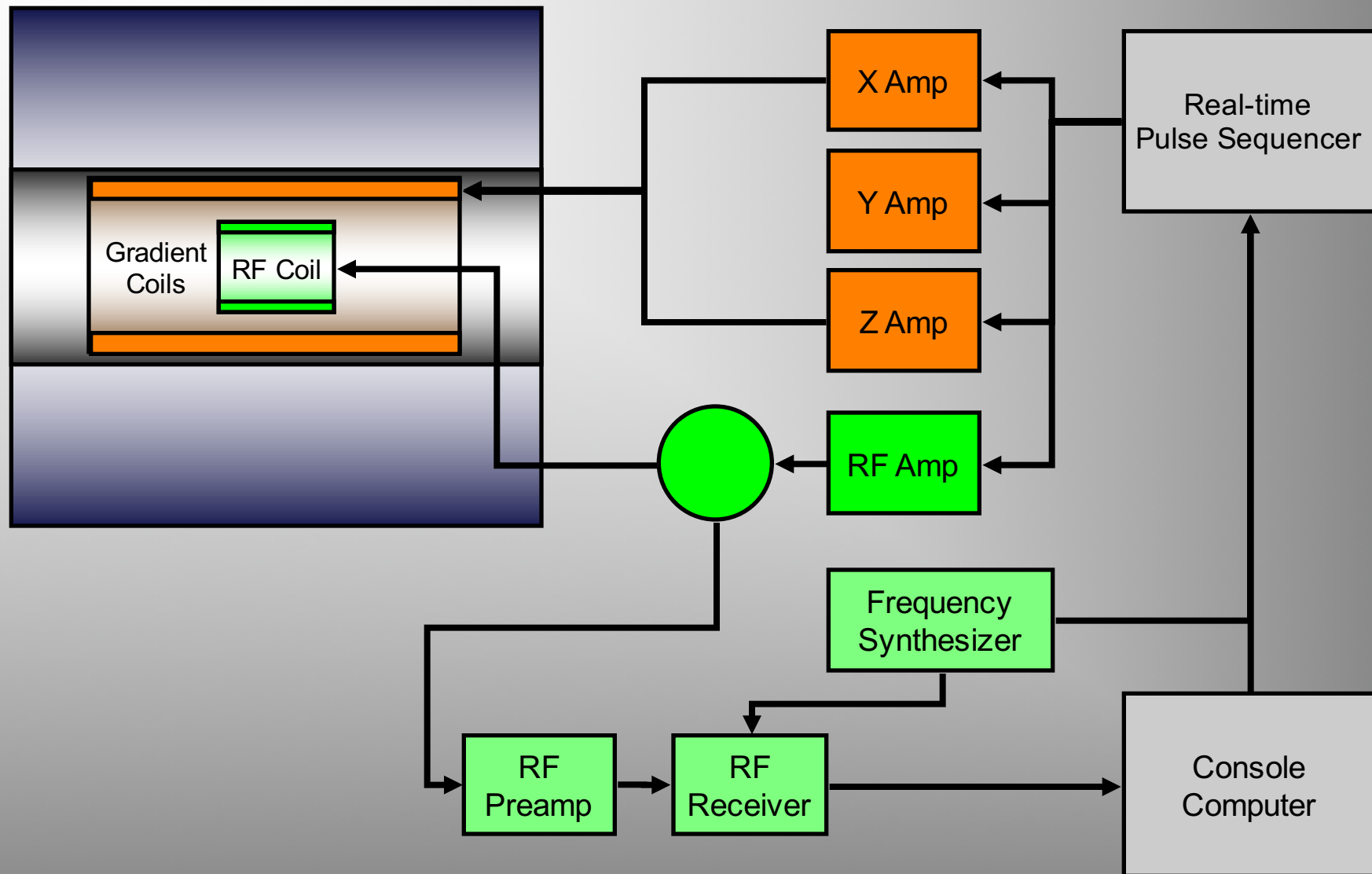
Pulse Programming Bootcamp 2005

Caltech Brain Imaging Center

California Institute of Technology

MRI Hardware

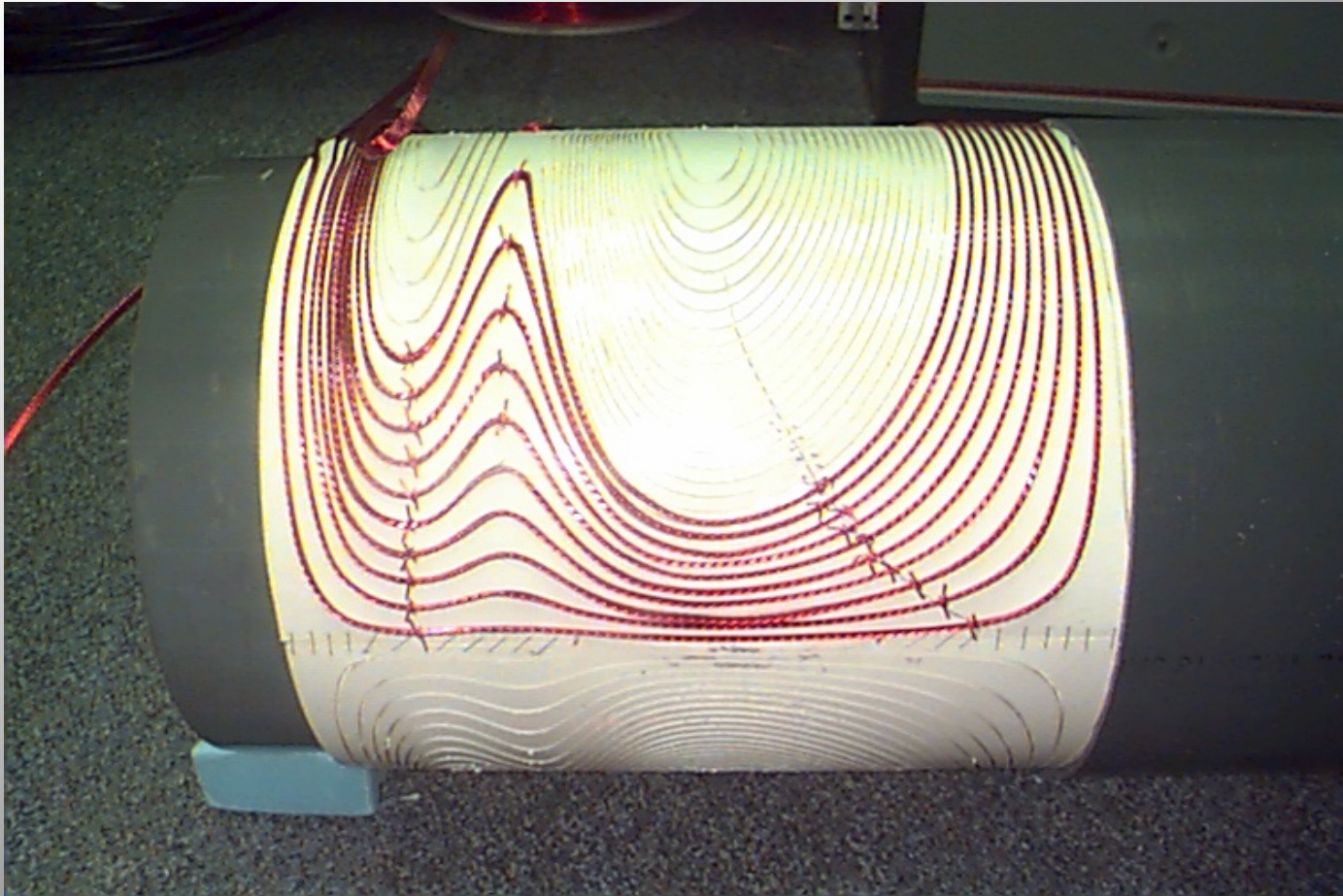
MRI Hardware Schematic



Magnet Solenoid

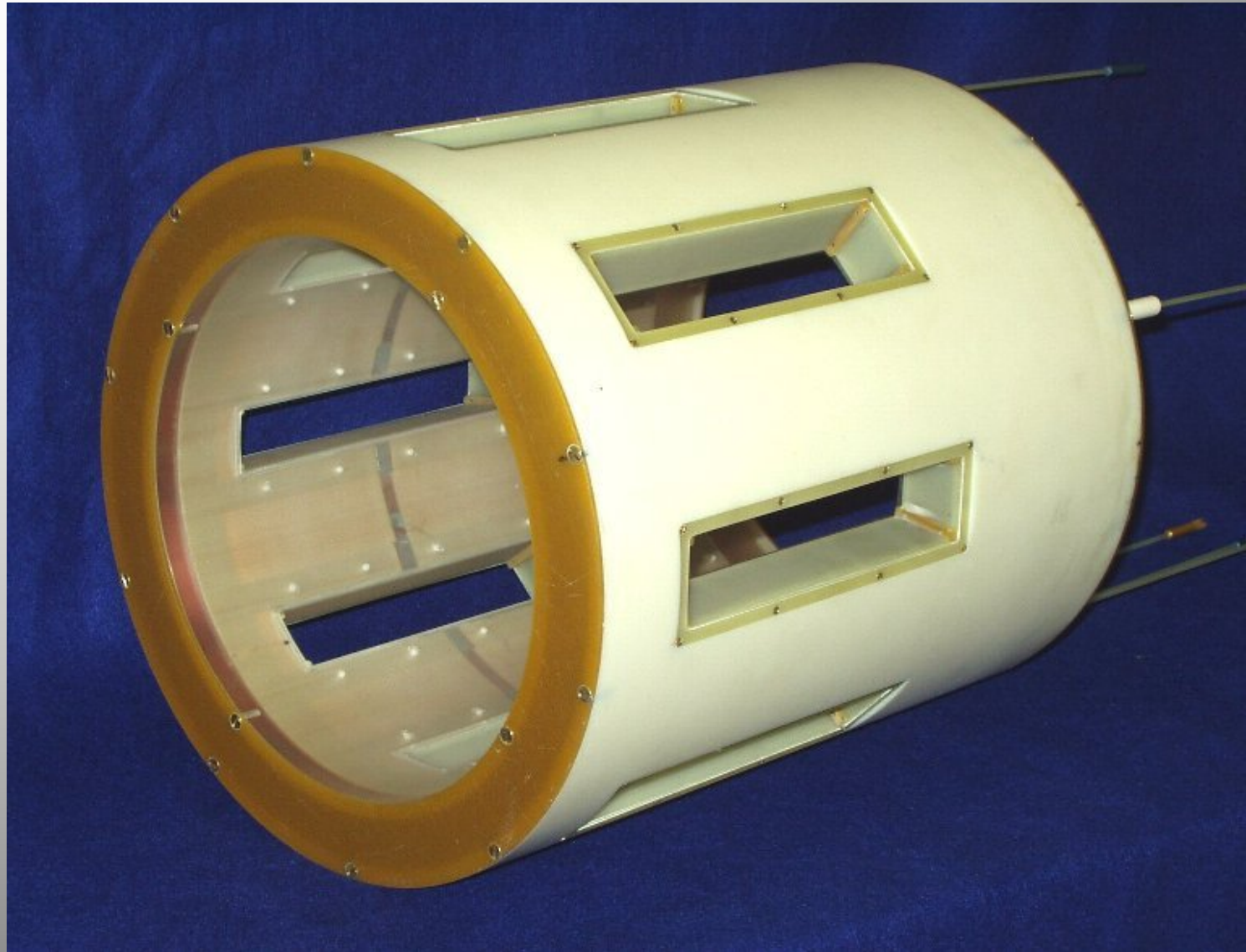


Gradient Coils

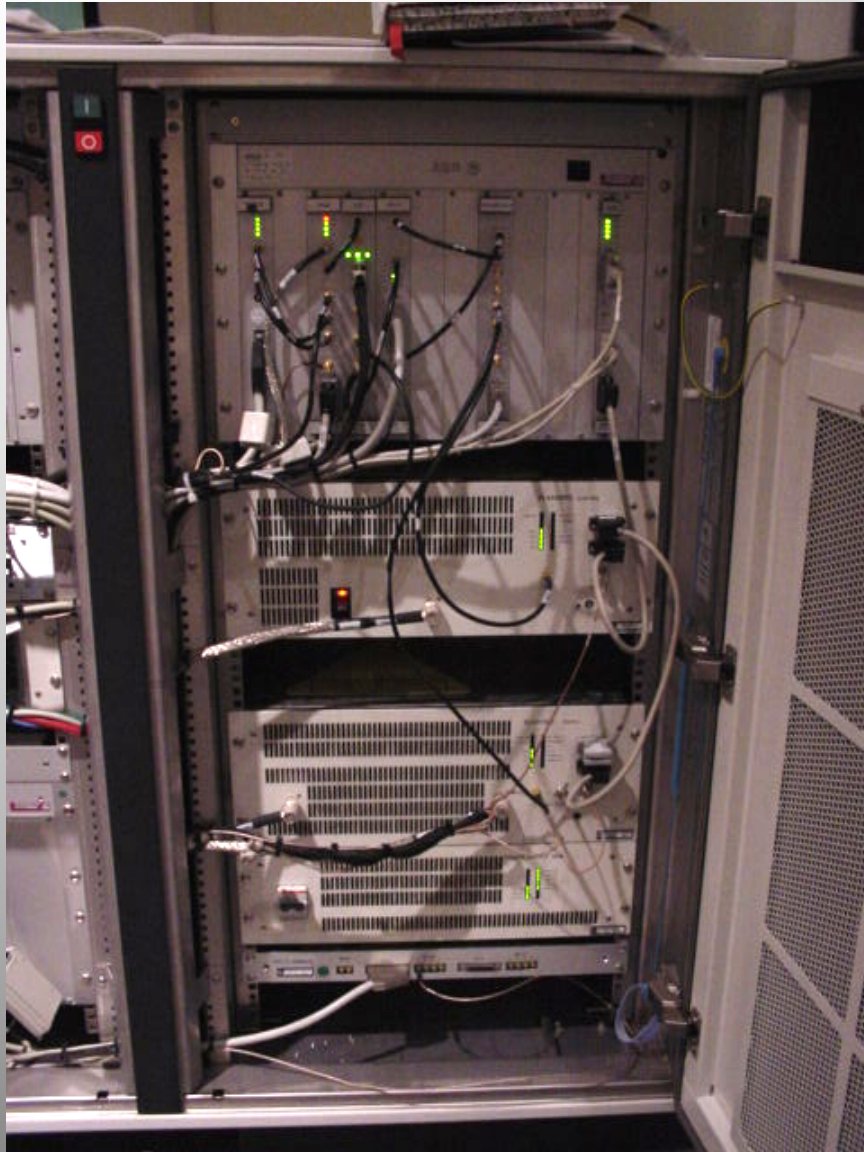


Chronik B, **Rutt BK**: Constrained Length Minimum Inductance Gradient Coil
Design. Magnetic Resonance in Medicine. 39 :270-278, 1998

RF Coils



System Electronics



Pulse Sequence Programs

Example Pulse Sequence Code

```
Microsoft Development Environment [design] - parsRelations.c
File Edit View Debug Tools Window Help
No

parsRelations.c
/*****
 * TR relations
 *****/

void BIC_FLASH_TR_Rels( void )
{
    int dim;
    double TotalTime;

    DB_MSG(("--->BIC_FLASH_TR_Rels\n"));

    TotalTime = 0.0;

    if( PVM_ErrorDetected == Yes )
    {
        UT_ReportError("FLASH-backbone: In function call!");
        return;
    }

    BIC_FLASH_MinTR();

    /*****
     * Calculate Total Scan Time and Set for Scan Editor
     *****/

    dim = PTB_GetSpatDim();

    /* Include segment loop */
    if (dim > 1)
        TotalTime = (int)(PVM_RepetitionTime * PVM_Matrix[1] * PVM_AntiAlias[1])
        * PVM_NAverages;

    /* Include 3D phase encoding loop */
    if (dim > 2)
        TotalTime *= PVM_Matrix[2] * PVM_AntiAlias[2];

    /* Include experiment repetitions */
    TotalTime *= PVM_NRepetitions;

    /* Update scan time string with total time */
    UT_ScanTimeStr(PVM_ScanTimeStr, TotalTime);

    PervDataShowInEditor("PVM_ScanTimeStr");
}
```

```
Microsoft Development Environment [design] - bic_flash.txt
File Edit View Debug Tools Window Help
No

bic_flash.txt
;-----
; START OF MAIN SEQUENCE
;-----

start,      10u

;-----
; Slice loop start
;-----

slice,      10u fq8b:f1

#include <TriggerPerSlice.mod>

;-----
; Magnetization preparation modules
;-----

prep,      10u

#include <SatSlices.mod>
#include <FatSup.mod>

; Set transmit frequency from list

    10u fq1:f1

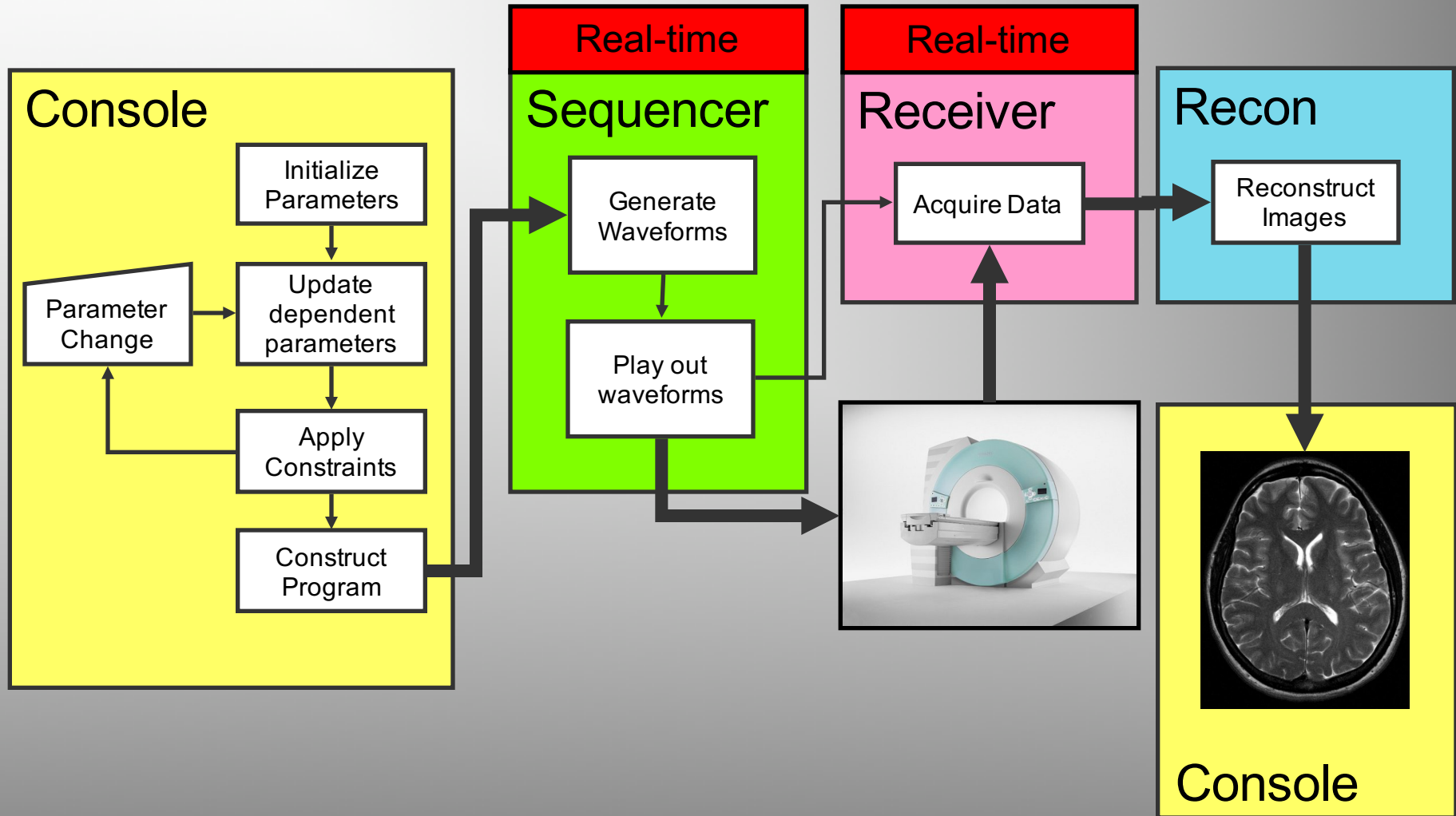
;-----
; Slice selection
;-----

d3  grad( {0} | {0} | {t0} )
d8  gatepulse 1
p0:sp0  ph0

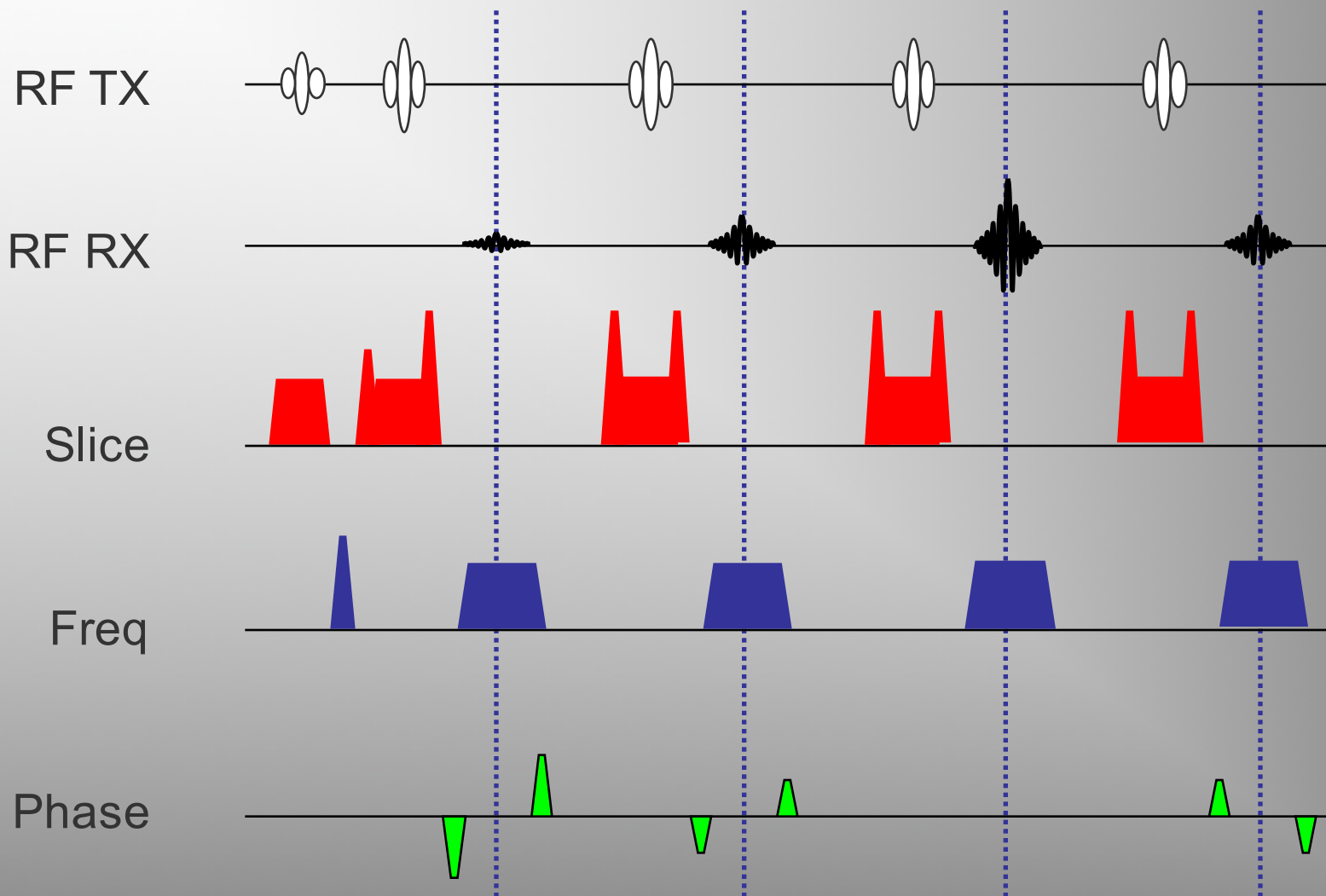
if (BIC_FLASH_UseMinTE == No)
{
    d4  groff          ; Switch of gradients
    d2              ; Allow variable TE
}

;-----
; Dead database phase encode and slice rephase
```

Pulse Program Flow



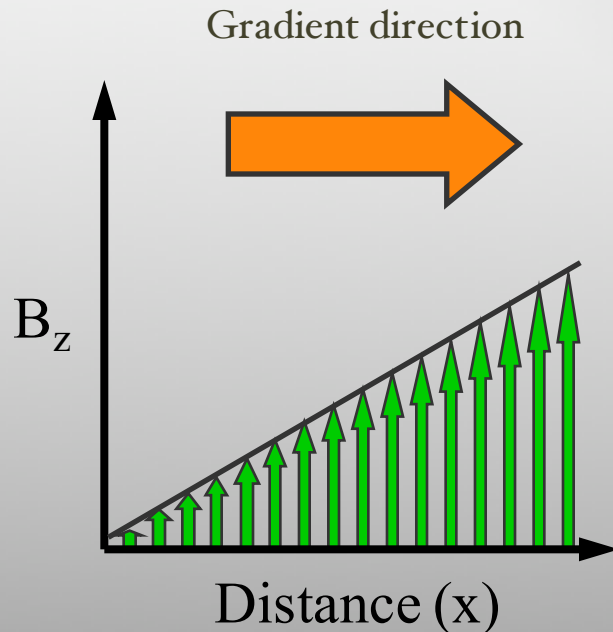
Pulse Sequence Diagrams



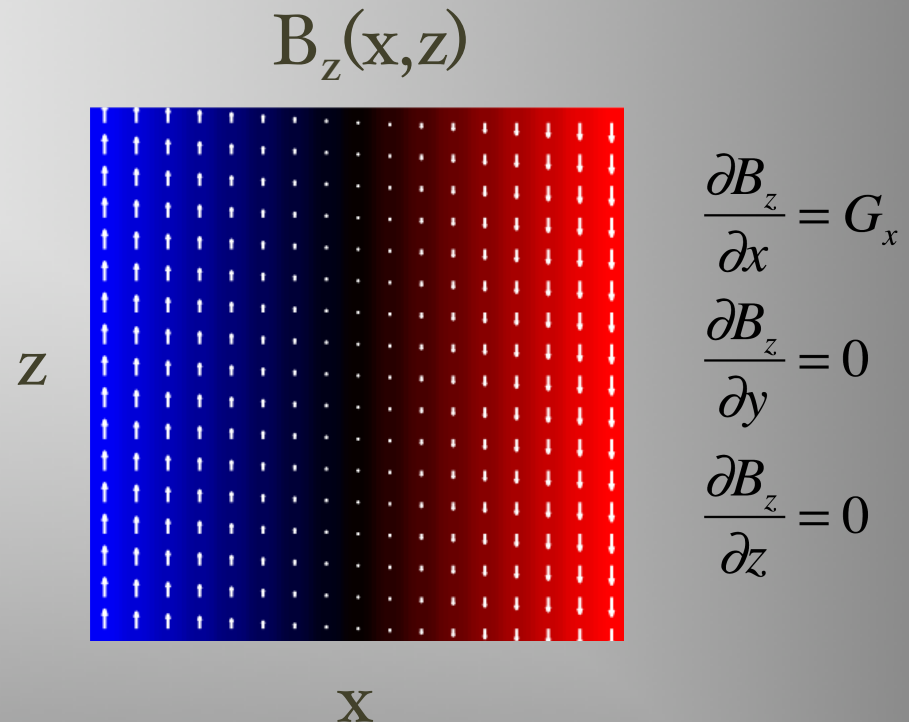
Gradient Pulses

Linear Magnetic Field Gradients

One-Dimensional



Two-Dimensional

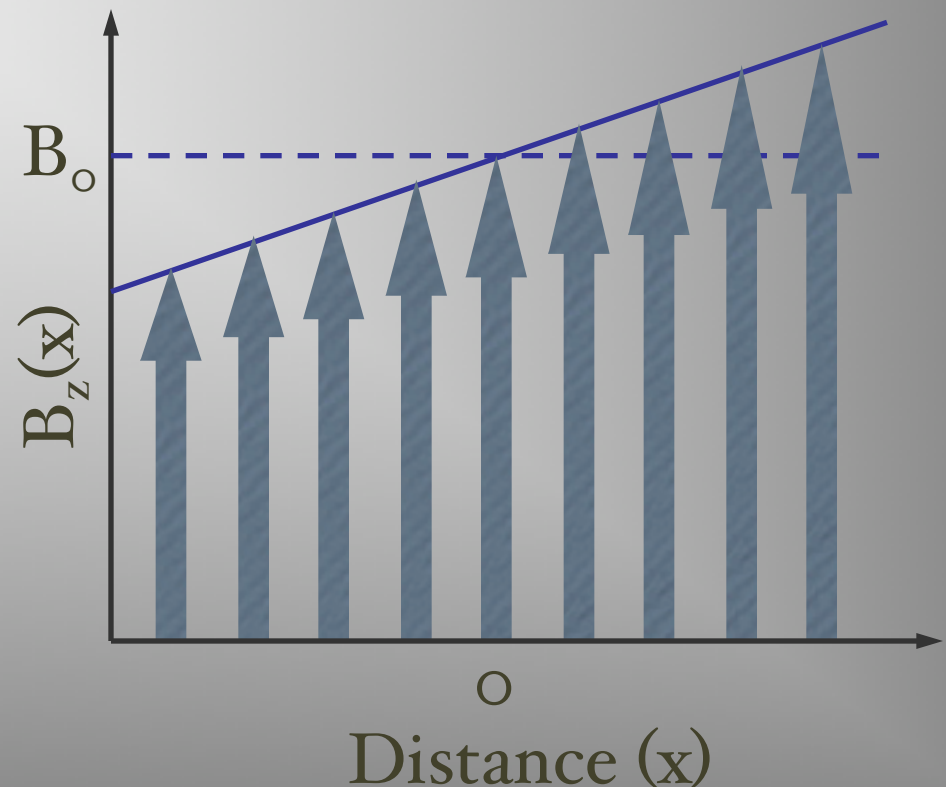


Deviation from B_0 typically very small ($\sim 0.1\%$)

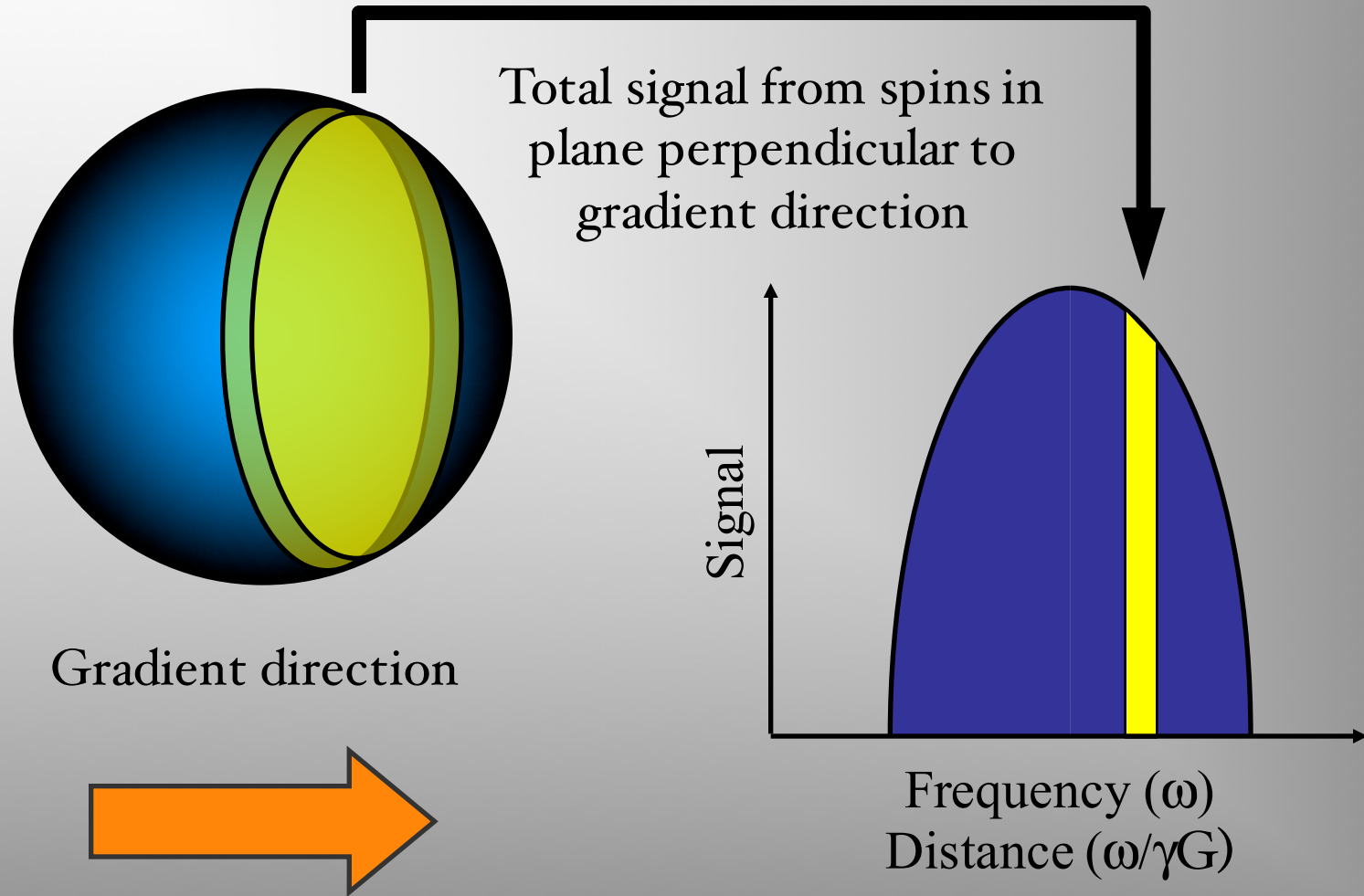
Field Gradients and Magnetization Phase

$$B_z(x) = B_0 + G_x x$$

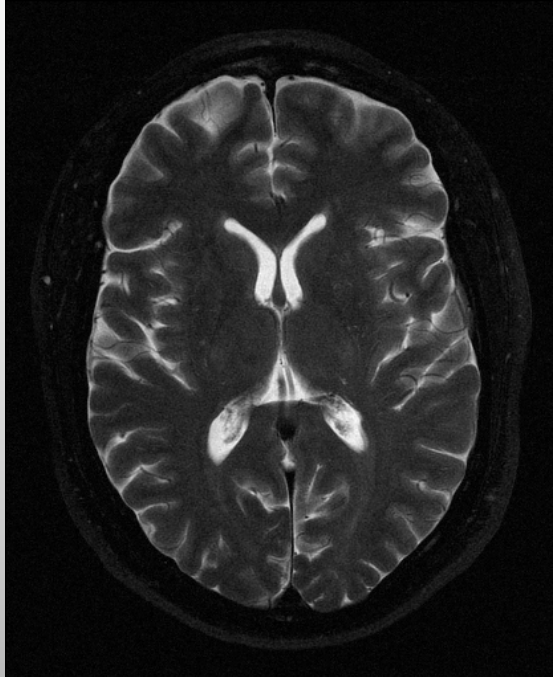
$$\begin{aligned}\phi(x, t) &= \omega(x) t \\ &= \gamma B_z(x) t \\ &= \gamma G_x x t\end{aligned}$$



Frequency Encoding



Frequency Encoding Bandwidth

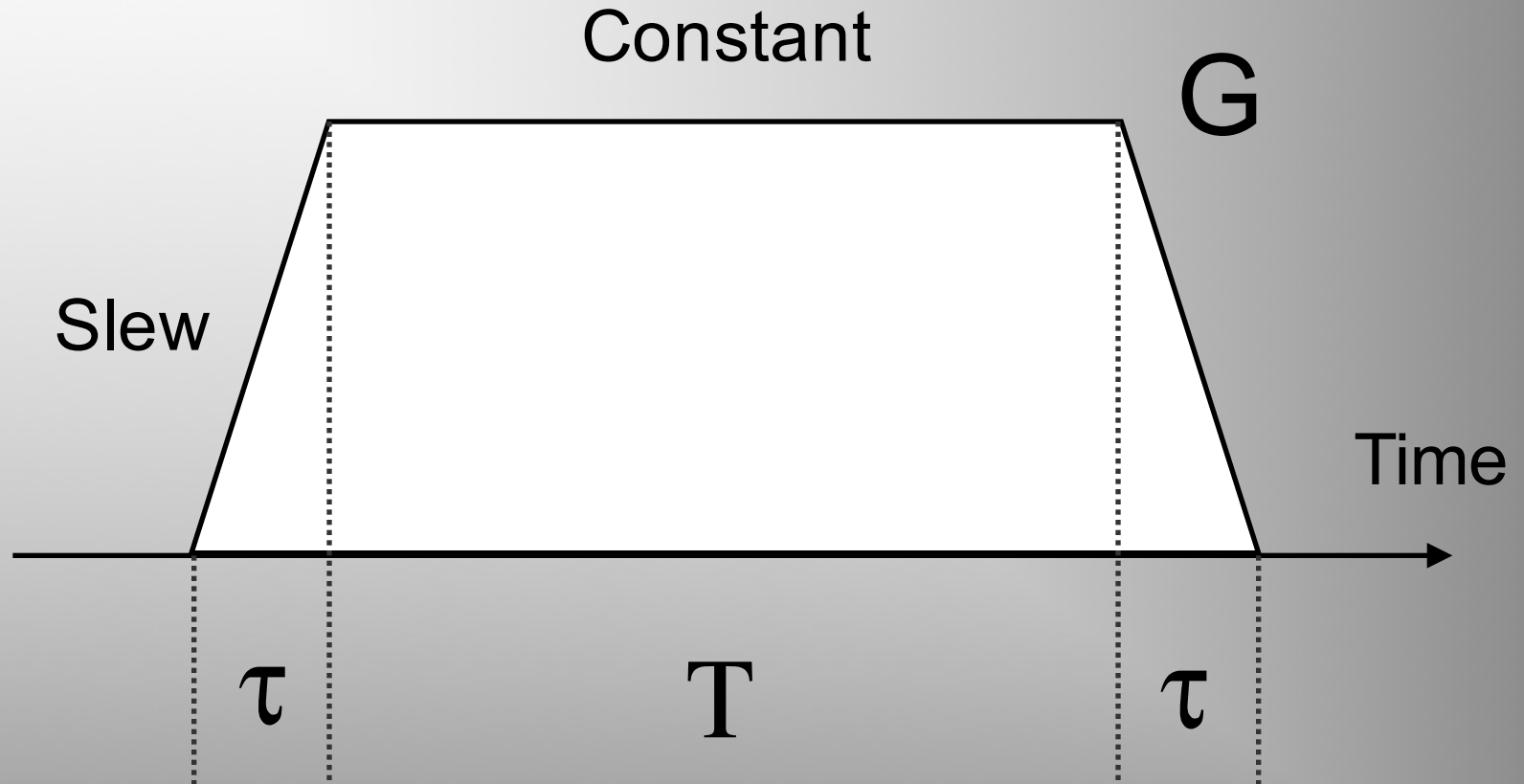


$$BW = \gamma G_x FOV_x$$

$$[Hz] = \left[\frac{Hz}{G} \right] \left[\frac{G}{cm} \right] [cm]$$

$$B_z = B_0 + G_x x$$

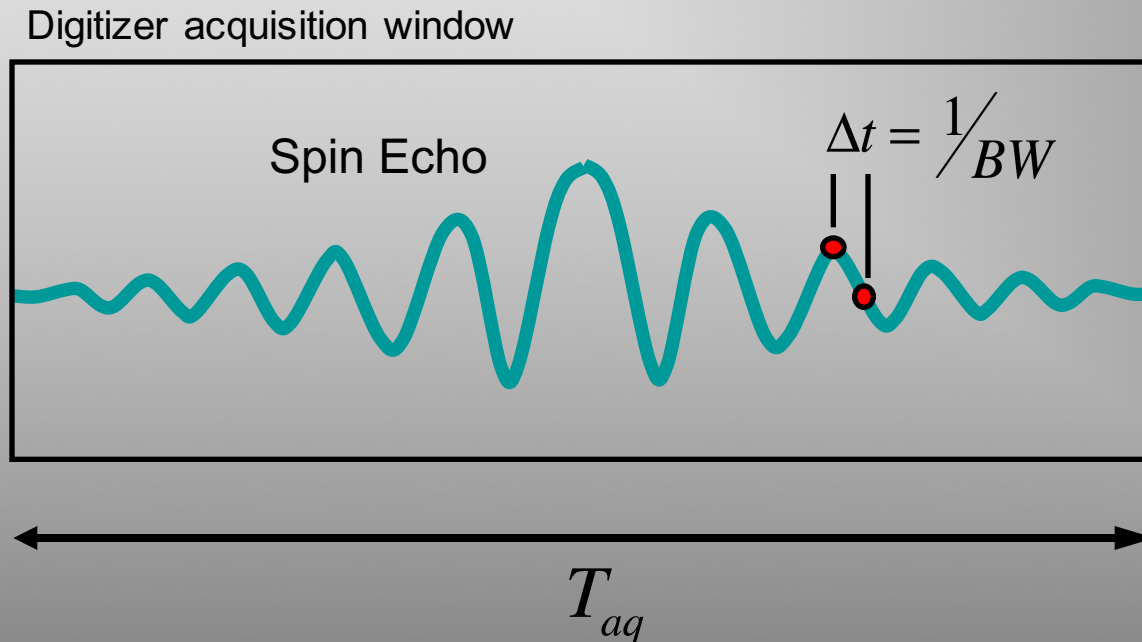
Real Gradient Pulses



Frequency Encoding Bandwidth and Noise

SNR is proportional to the square-root of the total digitizer acquisition time (c.f. SNR proportional to the square root of the number of signal averages).

$$\frac{S}{N} \propto \sqrt{T_{aq}} = \sqrt{N_x \Delta t} = \sqrt{\frac{N_x}{BW}}$$



Gradient Moments

k-space

k measures phase accumulated per unit distance over a time interval (radians/m) due to a time varying gradient (pulse, waveform, etc).

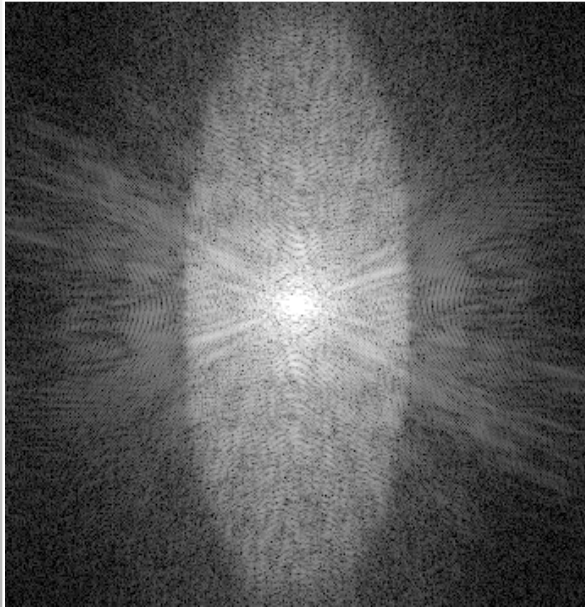
$$\mathbf{k}(t) = \int_0^t dt' \gamma \mathbf{G}(t')$$

k is a vector => k-space can be multidimensional.

The components of **k** (k_x , k_y , etc.) have units of radians/m.

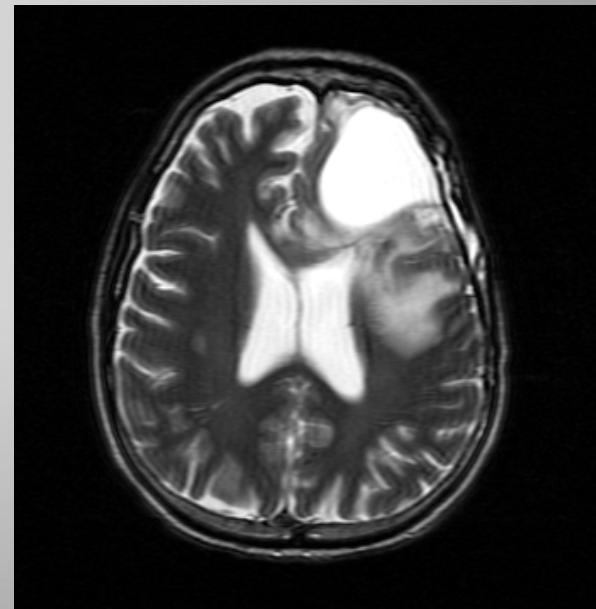
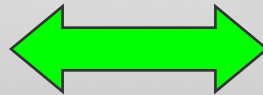
MR Imaging as Diffraction

MRI data is acquired in the inverse space of the final image



k-space

Fourier
Transform

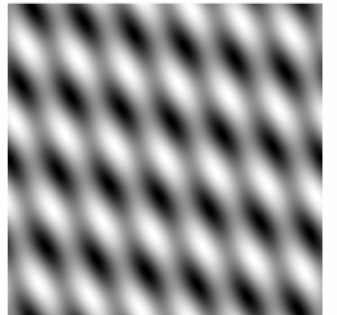
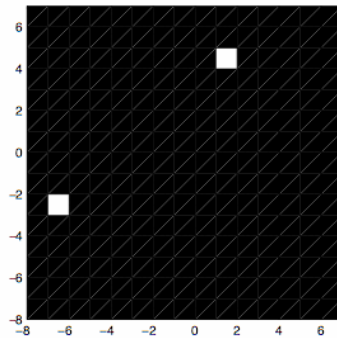
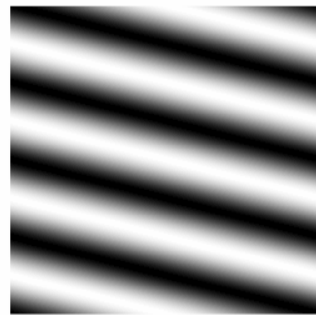
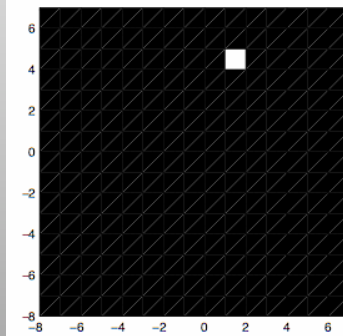
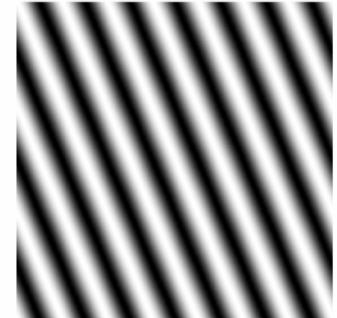
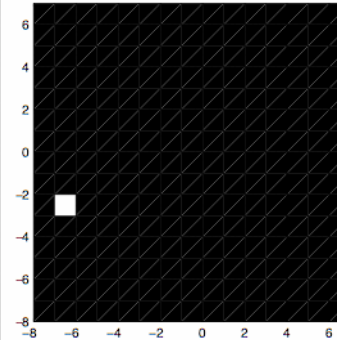
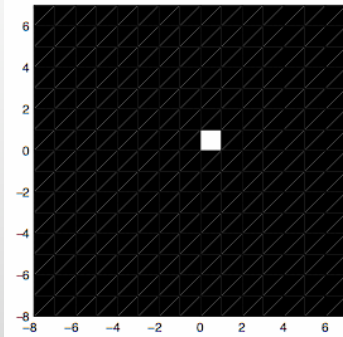


Frequency Encoded
Space

Spatial Frequencies and k-space

k-space

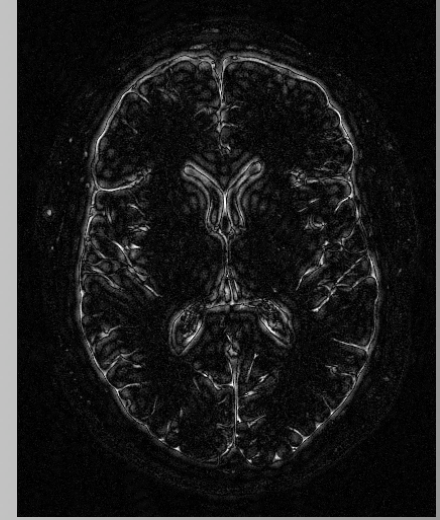
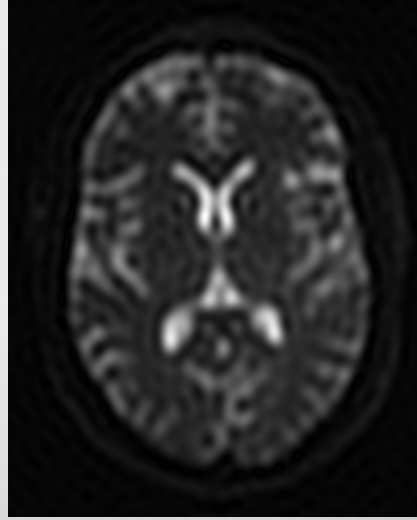
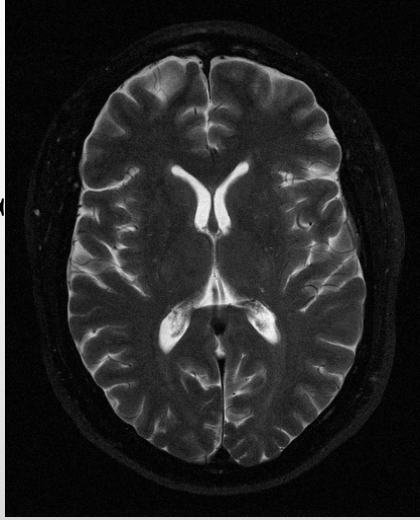
Real space



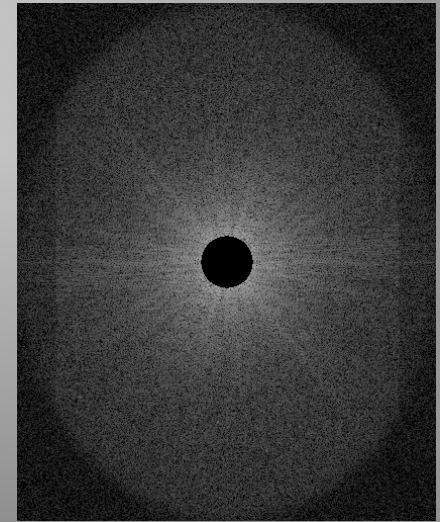
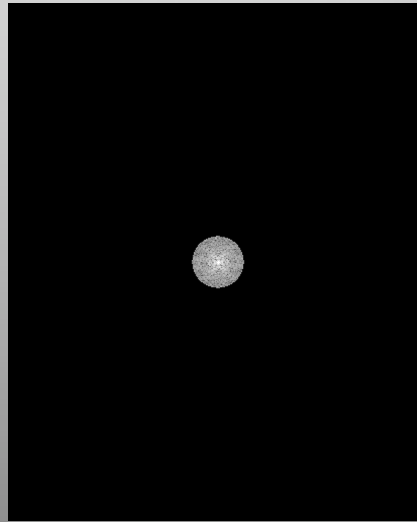
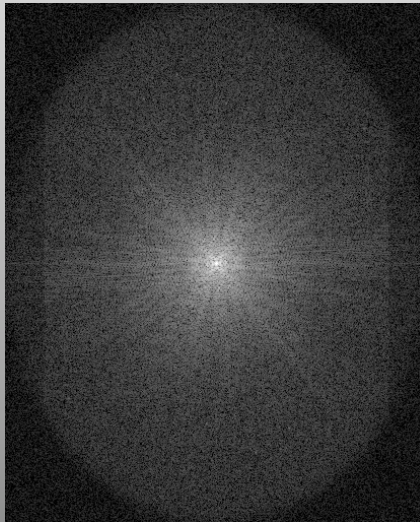
Coordinates in k-space equate to spatial frequency.

k-space Spatial Frequency Regions

Real Space



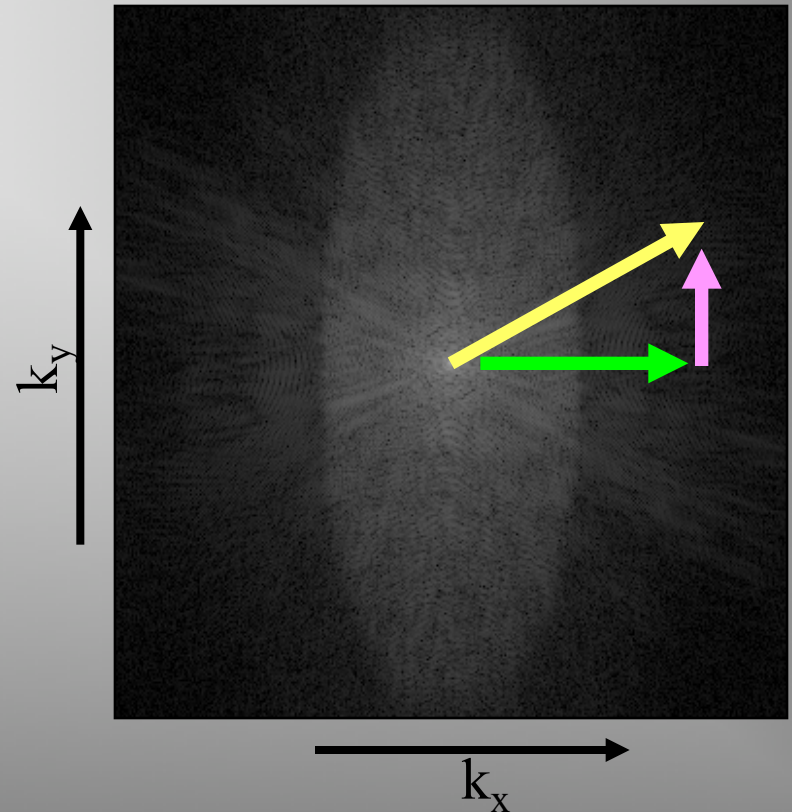
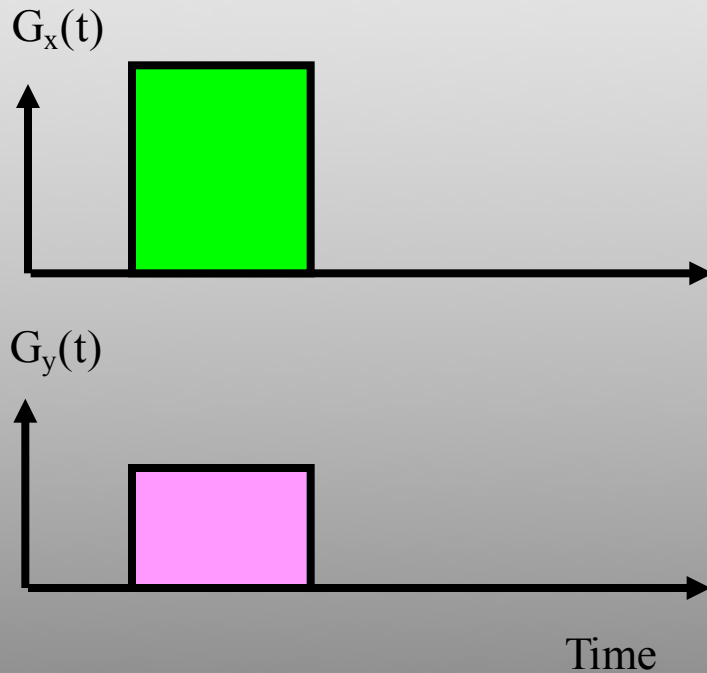
k Space



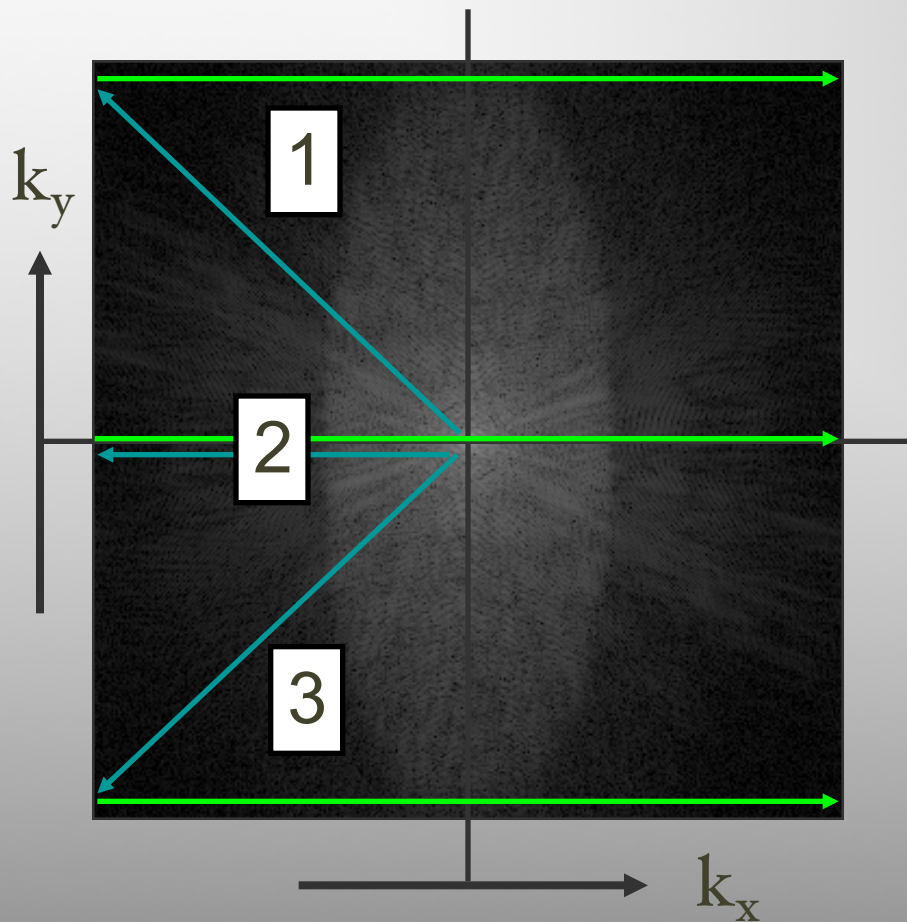
k-space Maneuvers

$$\mathbf{k}(t) = \int_0^t dt' \gamma \mathbf{G}(t')$$

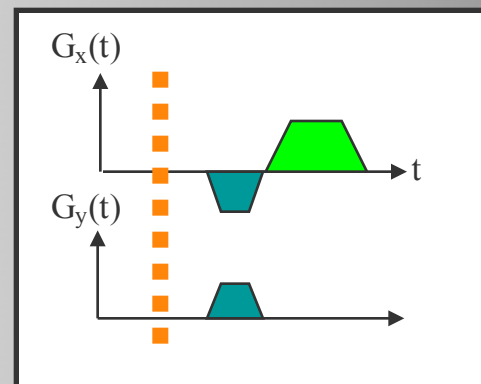
Gradient pulses move the spin system in k-space.



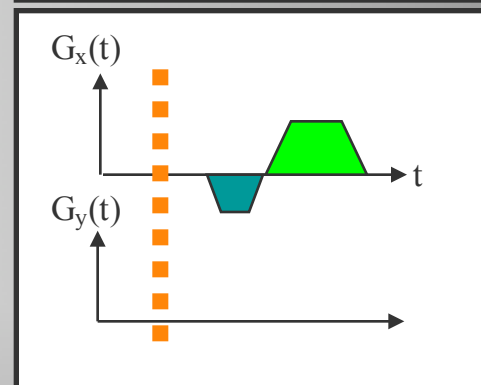
k-space Trajectories



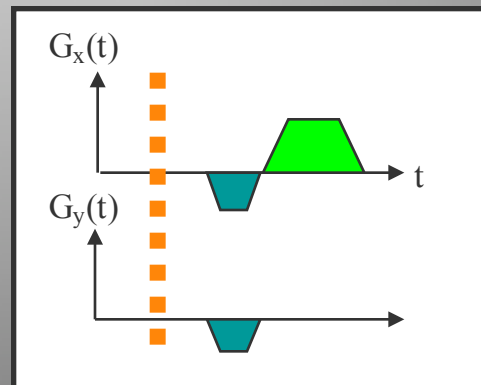
1



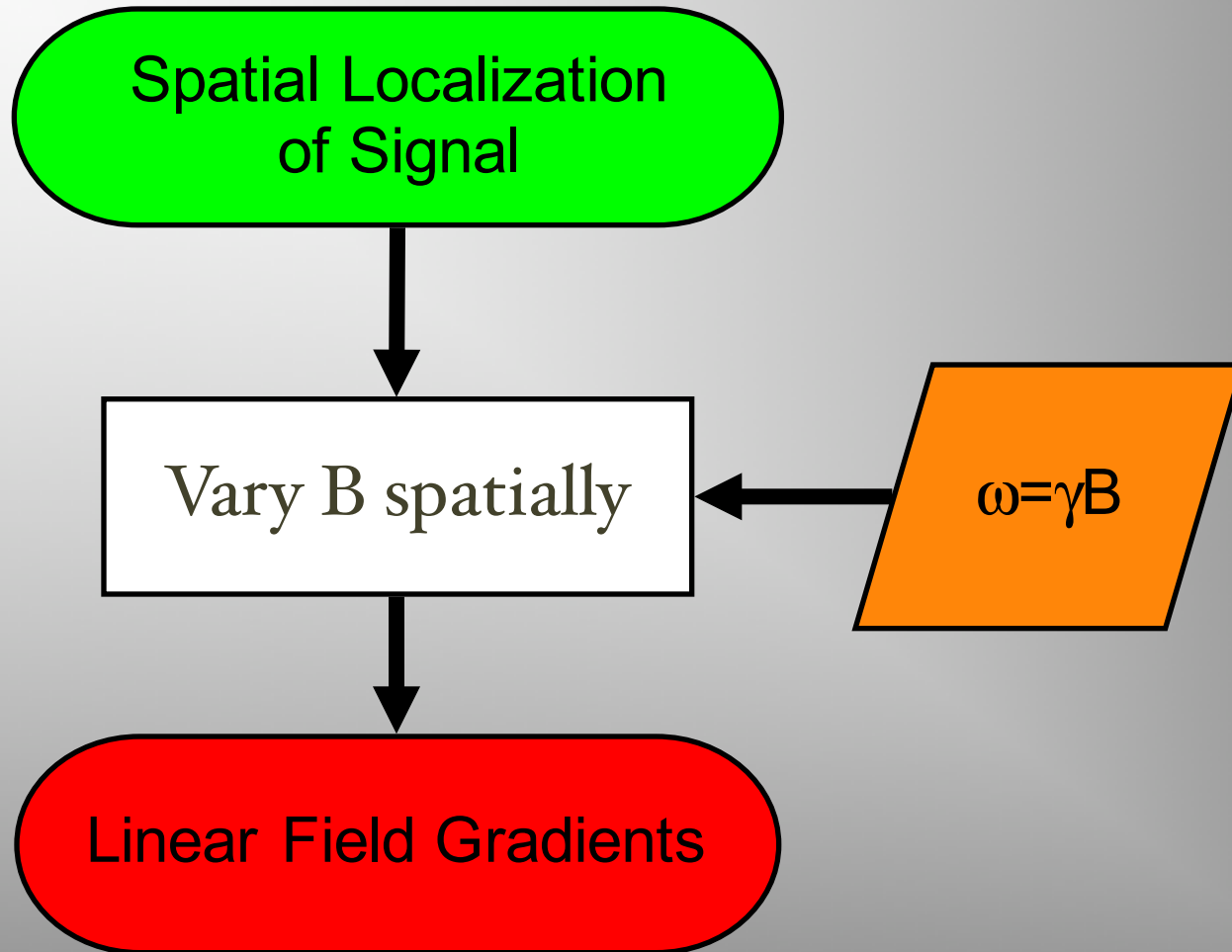
2



3



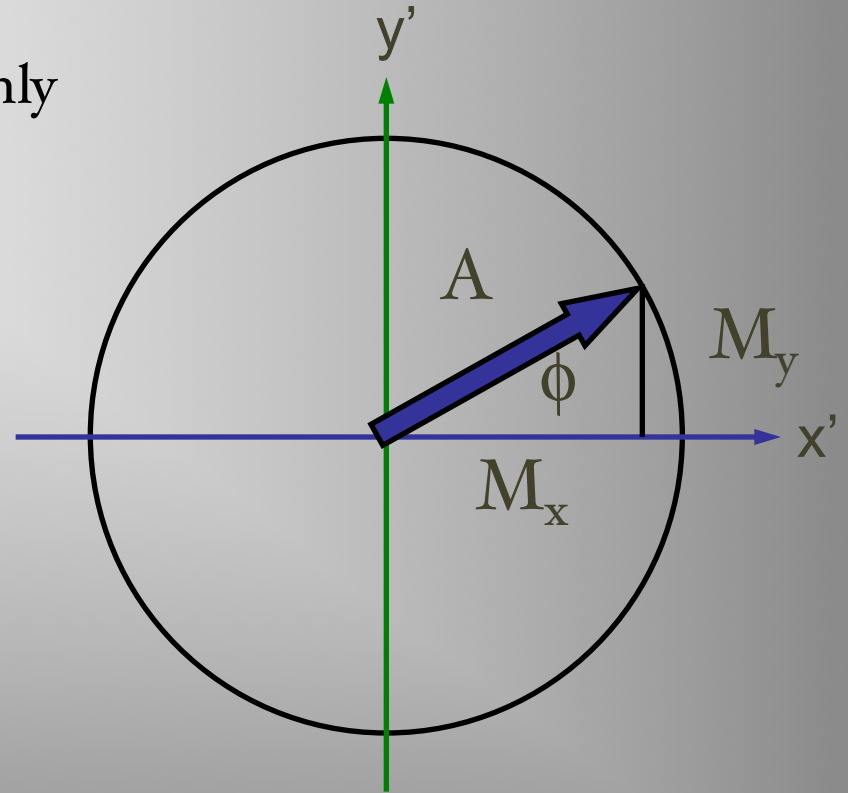
Spatial Encoding



MR Signal as a Complex Quantity

- Both the magnitude and phase of the MR signal are measured.
- Two signal channels are commonly referred to as “real” and “imaginary”.

$$\begin{aligned}M &= Ae^{i\phi} \\&= A\cos(\phi) + iA\sin(\phi) \\&= M_x + iM_y\end{aligned}$$



The Fourier Transform (FT)

The Fourier Transform is an Integral Transform which, for MRI, relates a time varying waveform to the corresponding frequency spectrum.

FORWARD TRANSFORM (time $\rightarrow$ frequency)

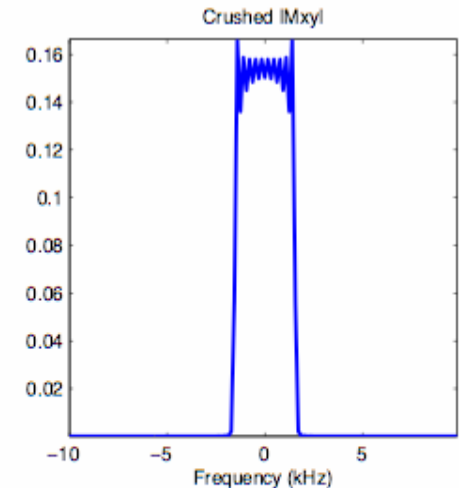
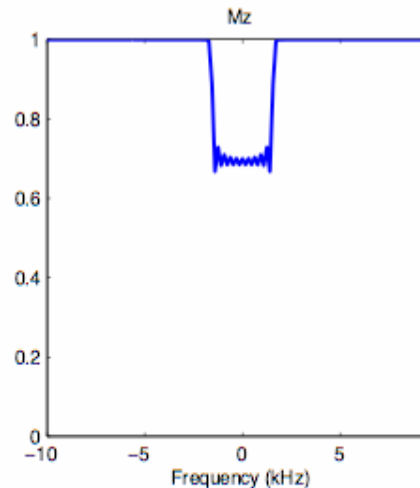
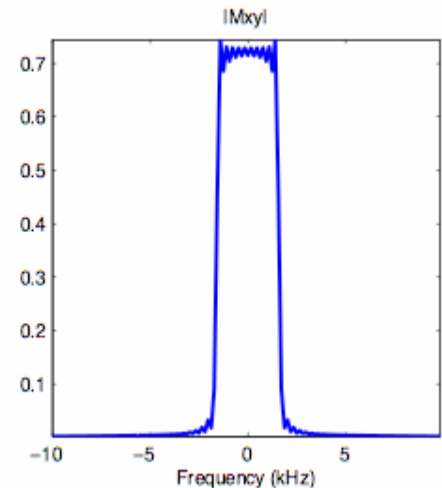
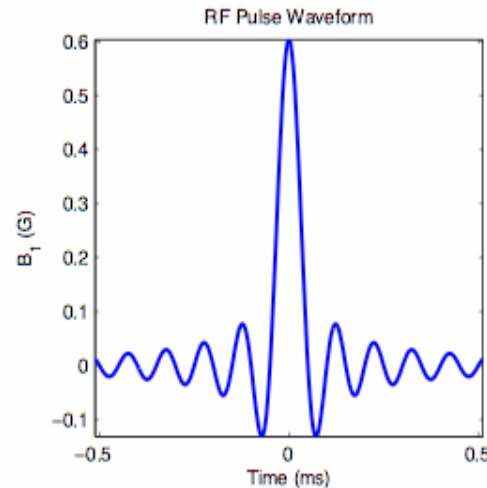
$$\bar{S}(\omega) = \frac{1}{\sqrt{2\pi}} \int_{-\infty}^{\infty} dt S(t) e^{i\omega t}$$

REVERSE TRANSFORM (frequency $\rightarrow$ time)

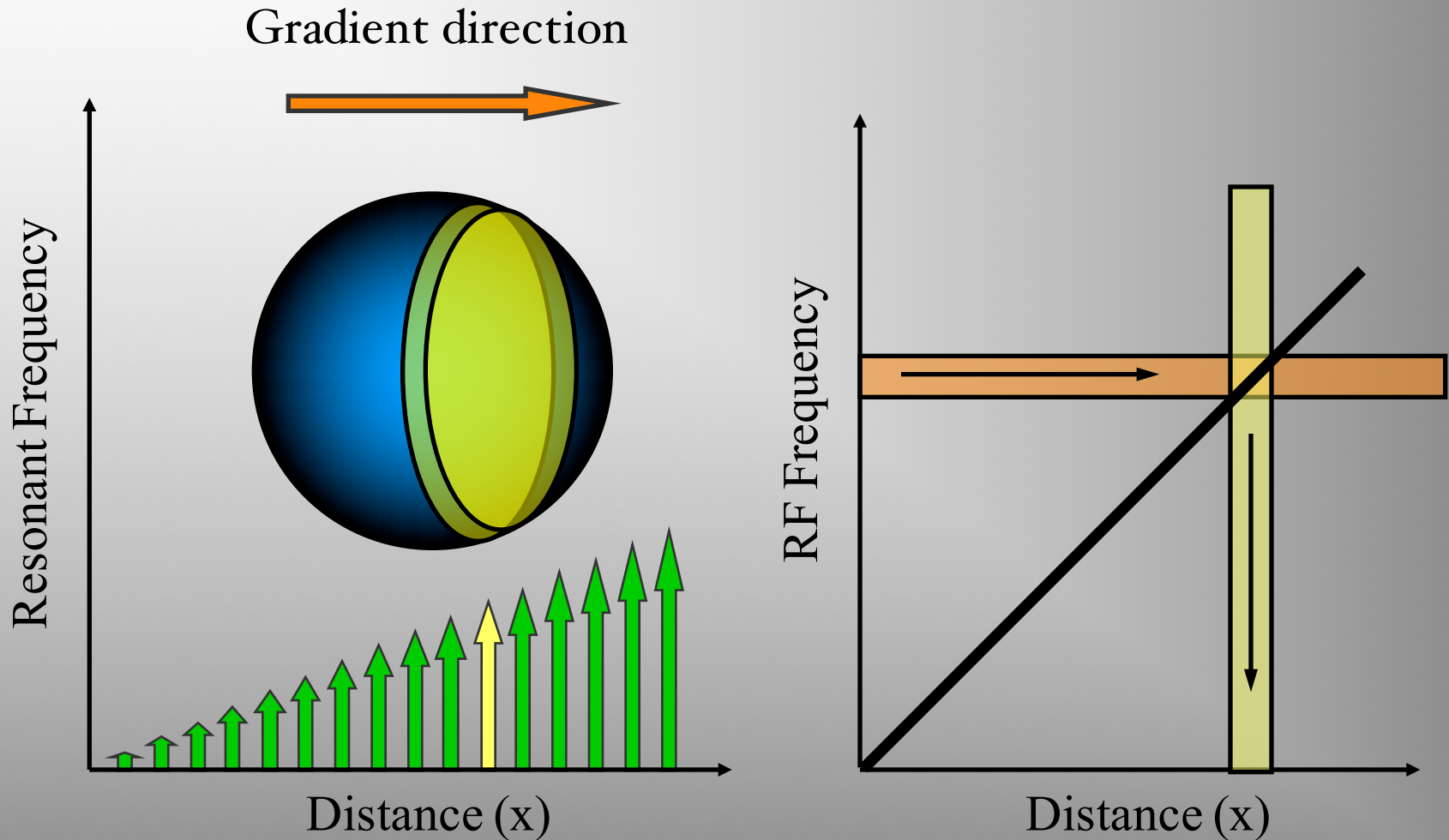
$$S(t) = \frac{1}{\sqrt{2\pi}} \int_{-\infty}^{\infty} dt \bar{S}(\omega) e^{-i\omega t}$$

Bandlimited RF Pulses

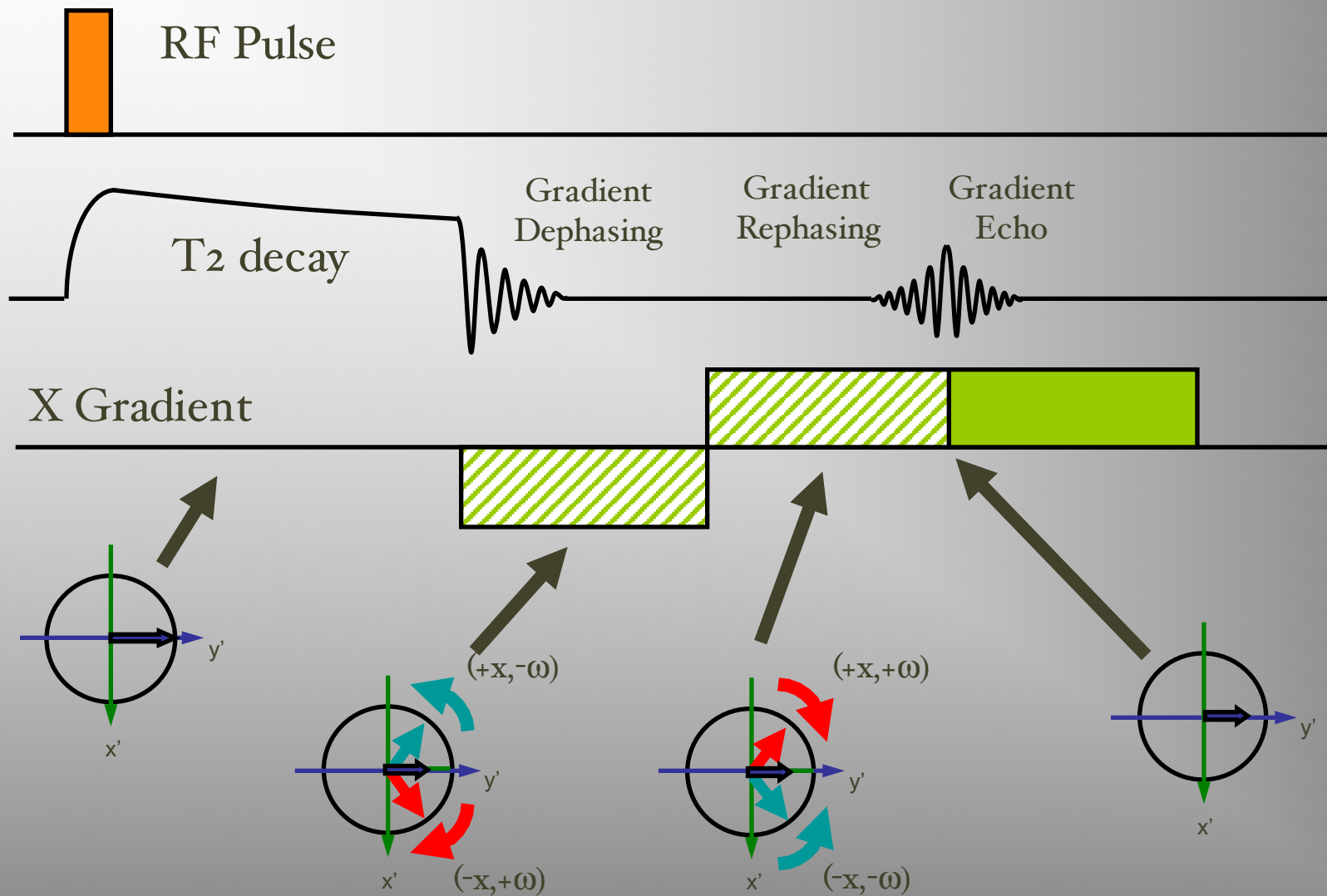
- Pulse waveform modulates Larmor carrier frequency.
- Affects frequency band centered on Larmor frequency.



Slice Selection with Gradients



The Gradient Echo



Construct Full Gradient Echo Sequence

Tomorrow : Pulse Sequences